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**(54) AN ENDOVASCULAR GRAFT PROSTHESIS AND KIT FOR IMPLANTATION OF SUCH A PROSTHESIS**

ENDOVASKULÄRES TRANSPLANTAT UND KIT ZUM IMPLANTIEREN EINES SOLCHEN TRANSPLANTATS

PROTHESE POUR GREFFE ENDOVASCULAIRE ET ENSEMBLE POUR L'IMPLANTATION

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## Description

[0001] An endovascular graft prosthesis and a kit for implantation of such a prosthesis.

[0002] The invention relates to an endovascular graft prosthesis for arrangement at or in the vicinity of a bifurcation in the arterial system of a patient and comprising a substantially tubular main body for location in an upstream artery above the bifurcation and substantially tubular legs joining said main body and extending via the bifurcation into each of two downstream branch arteries, said main body being made of a flexible microporous and surgically implantable woven material unpenetratable to blood.

[0003] In particular, the invention is concerned with the repair of an aneurysm in the vicinity of the aortic bifurcation, but it may also be applied to other parts of the arterial system where a principal upstream artery bifurcates into two branch arteries.

[0004] In order to prevent an aortic aneurysm, in particular in the lower part of the aorta close to the aortic bifurcation from causing a dangerous rupture of the aortic wall it is known to deploy a graft prosthesis in the region of the vessel affected by such an aneurysm.

[0005] An aortic aneurysm may develop as a result of a reduction of the strength of the aortic wall whereby the diameter of the affected part of the aorta may increase to more than 5 cm. Such expansions may result in flow irregularities and promotion of deposits of coagulated blood in the affected region. At increased expansion the remaining strength of the aortic wall will naturally decrease and may ultimately result in rupture of the vessel with an inherent danger of acute bleeding.

[0006] With conventional prior art endovascular prosthesis for aortic implantation surgical opening of the actual vascular section will be necessary for deployment of the prosthesis. For this purpose a partial cut is made in the wall of the aneurysm to introduce the prosthesis formed as an integral unit of a plastic material and secure it by sewing.

[0007] From EP-A-0508473 and EP-A-0539237 bifurcated graft prosthesis are known which may be transluminarily implanted for the repair of an aneurysm at or in the vicinity of the aortic bifurcation. In both cases the bifurcated prosthesis is made as an integral unit with a main body and two tubular legs joining the main body in a bifurcation. Due to this design the implantation operation becomes relatively complicated since the integral unit must be introduced through one of the iliac arteries with one of the legs in a fold-over condition until the graft is disposed proximal of the aortic bifurcation following which the proximal extremity of the prosthesis must be secured upstream of the actual vascular section and the folded over leg must be pulled down into the other iliac artery.

[0008] It is the object of the invention to provide an endovascular graft prosthesis of the kind set forth for transluminal implantation at the aortic bifurcation by a

considerably simpler implantation operation than the above-mentioned prior art solutions.

[0009] In order to achieve this an endovascular graft prosthesis according to the invention is characterized in that the main body is substantially bag-shaped with an open proximal upstream end and a distal downstream bottom region in which two outlet openings are provided, said main body being radially expandable and attachable in a radially expanded condition to the inner side of said upstream artery upstream of the bifurcation by fixation means, said legs being made as separate resilient and radially expandable leg stent devices adapted for introduction in a collapsed condition through said branch arteries and into said outlet openings, each of said stent devices being engageable in its radially expanded condition against the rim of the corresponding outlet opening to provide a leakage-free bifurcated graft prosthesis.

[0010] By making up the prosthesis from a number of separate components which may be sequentially introduced in the arterial system by percutaneous operations through small openings with a punctual diameter up to 5 mm the components may be endovascularly assembled to a complete prosthesis after deployment in the actual vascular section. Thereby, the prosthesis according to the invention may also be applied for repair of an aneurysm extending into the iliac arteries.

[0011] The endovascular graft prosthesis according to the invention can be arranged at or in the vicinity of a bifurcation in the arterial system of a patient and associated branch arteries by the steps of introducing through a first branch artery in an upstream direction by means of a first guide wire a separate, radially expandable and substantially bag shaped main body into an upstream artery to extend into a region thereof above the bifurcation, said main body having an open proximal upstream end with associated fixation means and a distal downstream bottom region in which two outlet openings are provided, expanding said main body radially in said upstream artery with said proximal end attached to the wall thereof, and introducing by means of further guide wires a radially expandable leg stent device through each of the branch arteries into each of said outlet openings.

[0012] The invention also relates to a kit comprising an endovascular graft prosthesis as defined in any of claims 1 - 5, said kit further comprising a first guide wire for use in introducing said main body into an upstream artery through a first branch artery in an upstream direction to extend into a region of the upstream artery above the bifurcation, and for possible use in introducing a catheter through each of the branch arteries over each end of the guide wire prior to the removal thereof.

[0013] Further embodiments of the kit according to the invention are described in claims 7 and 8.

[0014] Using this kit the main body consisting of a microporous woven material unpenetratable to blood

may be guided by means of the first guide wire from a puncture in an iliac artery into the aorta and deployed there with a downstream orientation of the distal bottom region of the body with respect to the blood flow direction. Thereby, the guide wire will be coaxially located in one or both of the outlet openings of the bag-shaped body. In spite of the two outlet openings the main body will be sufficiently expanded by the blood flow in its bottom region. In this condition, the main body is secured to the inner wall of the aorta upstream of the bifurcation by means of a radially expandable stent device which may typically be a self-expandable metallic stent. Following subsequent introduction of guide wires through the two outlet openings and across the lumen of the stent device a leg stent device may be introduced over each guide wire to extend at least through the distance between the bottom region of the main body and the junction of the iliac arteries. The leg stent devices forming separate components of the prosthesis may have an elastic covering over their entire length and are also radially expandable.

[0015] The introduction of the two leg stent devices which may also be self-expandable metallic stents may take place by use of conventional catheter technique whereby the guide wire and the catheter are guided from one outlet opening through the other and into the opposite iliac artery from where it may be guided in a conventional way through the vessel to the skin. By drawing of the curved guide wire extending through the outlet openings the position of the main body may still be corrected. Subsequently, two catheters may be introduced into the outlet openings over the guide wire thus positioned from the two groins to allow coaxial introduction of two guide wires to replace the two catheters. Subsequently the two leg stents covered by woven material are introduced over the positioned guide wires which can take place simultaneously for both stent devices.

[0016] In the expanded condition the two leg stents will press against the rim of the outlet openings and complete the main body into a leakage free endovascular prosthesis with a bifurcation secured in the aorta.

[0017] Preferably the main stent is attached to the bag-shaped main body with the downstream distal end overlapped by the upstream proximal end of the main body.

[0018] By a further development of the invention the endovascular deployment of the prosthesis may be substantially facilitated if the main stent device and the leg stent devices in a manner known per se are formed by self-expandable metal stents.

[0019] According to a further embodiment of the invention the rim of each outlet opening may diverge in the downstream direction.

[0020] By this measure there will be formed in each outlet opening close to the inner side of the bottom region of the bag-shaped main body a radially inwardly projecting opening rim against which the external side

of the leg stent may engage tightly whereby the security against leakage will be increased.

[0021] Further, according to an embodiment of the invention the maximum external diameter of each of the leg stents may be 2-4 mm greater than the minimum rim diameter of each outlet opening.

[0022] Thereby, the components may be connected in a sufficiently stable and leakage free manner without any requirement for additional means for this purpose.

[0023] The invention will be further explained with reference to an embodiment shown on the schematical drawing in which

fig. 1 shows a bag-shaped main body of a prosthesis according to the invention deployed in expanded condition within an aortic aneurysm,

fig. 2 illustrates the introduction of two guide wires into the main body of fig. 1 and

fig. 3 the main body completed with two leg stents into a prosthesis with a bifurcation.

[0024] As example of the application of the invention, figures 1 to 3 illustrate schematically an arterial system 1 in which the abdominal part of the aorta 2 extending between two branch arteries 3,4 leading to the kidneys and a bifurcation joining two iliac arteries 5,6 has been damaged by a balloon shaped aneurysm 7.

[0025] As illustrated in figure 1 a bag-shaped main body made of a micro-porous woven material unpenetrable to blood is first introduced in the region of the aneurysm 7 in the aorta 2, said main body having a bottom region with two outlet openings 9,10. The main body 8 is provided with a self-expandable metallic stent 11 and is introduced in contracted condition through an iliac artery 5 over a guide wire 12 and deployed in the aorta 2 in such a way that the metallic stent 11 will press at least the upper edge of the main body 8 tightly against the inner side of the aorta 2 above the aneurysm 7. In the bottom region of the main body 8 the guide wire 12 may as shown in dashed lines in fig. 1 be bent so as to allow it to be guided outwards through the outlet opening and the other iliac artery 6. Thereby a catheter not shown may be introduced over each of the free ends of the guide wire 12 until the main body 8 which has expanded due to the action of the blood flow. After removal of the guide wire 12 a single guide wire 13,14 may be introduced through each catheter to finalize the deployment preparation as illustrated in figure 2.

[0026] Over each of the guide wires 13,14 a self-expandable metallic stent 15,16 with an elastic covering may now be introduced in a conventional way. As illustrated in fig. 3 a proximal end part of each of the metallic stents 15,16 projects into the interior of the main body whereas a distal end part of each metallic stent projects relatively deep into the iliac arteries 5,6.

[0027] In the expanded condition illustrated in fig. 3 the metallic stents 15,16 are contracted in the rim region of each of outlet openings 9 and 10 and will thereby be

firmly and tightly connected with the main body 8. Thereby, the main body together with the leg stents 15 and 16 will form an endovascular aortic prosthesis overlapping the aneurysm 7 and being implantable by relatively simple percutaneous operations.

#### Claims

1. An endovascular graft prosthesis for arrangement at or in the vicinity of a bifurcation in the arterial system of a patient and comprising a substantially tubular main body (8) for location in an upstream artery (2) above the bifurcation and substantially tubular legs (15,16) joining said main body and being adapted to extend via the bifurcation into each of two downstream branch arteries (5,6) said main body being made of a flexible microporous and surgically implantable woven material unpenetratable to blood, characterized in that the main body (8) is substantially bag-shaped with an open proximal upstream end and a distal downstream bottom region in which two outlet openings (9, 10) are provided, said main body being radially expandable and attachable in a radially expanded condition to the inner side of said upstream artery (2) upstream of the bifurcation by fixation means (11), said legs being made as separate resilient and radially expandable leg stent devices (15, 16) adapted for introduction in a collapsed condition through said branch arteries and into said outlet openings (9,10), each of said stent devices (15, 16) being engageable in its radially expanded condition against the rim of the corresponding outlet opening to provide a leakage-free bifurcated graft prosthesis.
2. An endovascular graft prosthesis as claimed in claim 1, characterized in that said fixation means comprises a main stent device (11) which is attached to the bag-shaped main body (8) with a downstream distal end of the main stent device (11) overlapped by the upstream proximal end of the main body (8).
3. An endovascular graft prosthesis as claimed in claim 2, characterized in that said main stent device (11) and leg stent devices (15,16) are formed by expandable metal stents.
4. An endovascular graft prosthesis as claimed in claim 1, 2 or 3, characterized in that the rim of each outlet opening (9, 10) diverges in the downstream direction.
5. An endovascular graft prosthesis as claimed in claim 4, characterized in that the maximum external diameter of each of the leg stents (15, 16) is 2-4 mm greater than the minimum rim diameter of

each outlet opening (9, 10).

6. A kit comprising an endovascular graft prosthesis as defined in any of claims 1 - 5, said kit further comprising a first guide wire (12) for use in introducing said main body (8) into an upstream artery through a first branch artery (5) in an upstream direction to extend into a region of the upstream artery above the bifurcation, and for possible use in introducing a catheter through each of the branch arteries over each end of the guide wire prior to the removal thereof.
7. A kit according to claim 6, further comprising a catheter for introduction through each of the branch arteries over each end of said first guide wire (12) prior to removal thereof and for subsequent use in introduction of further guide wires for use in introduction of the leg stent devices (15, 16).
8. A kit according to claim 7, further comprising guide wires (13, 14) for use in introduction of the leg stent devices (15, 16).

#### Patentansprüche

1. Endovaskuläre Implantationsprothese zur Anordnung an oder in der Nähe einer Bifurkation im arteriellen System eines Patienten und umfassend einen im wesentlichen rohrförmigen Hauptkörper (8) zur Platzierung in einer stromaufwärts gelegenen Arterie (2) oberhalb der Bifurkation und im wesentlichen rohrförmigen Schenkeln (15, 16), die mit dem Hauptkörper verbunden und so ausgebildet sind, daß sie sich über die Bifurkation in jede von zwei stromabwärts gelegenen abzweigenden Arterien (5, 6) erstrecken, wobei der Hauptkörper aus einem elastischen mikroporösen und chirurgisch implantierbaren blutundurchlässigen Gewebe gebildet ist, dadurch gekennzeichnet, daß der Hauptkörper (8) im wesentlichen balgförmig mit einem offenen proximalen, stromaufwärts gelegenen Ende und einem distalen, stromabwärts gelegenen Bodenbereich ist, in dem zwei Auslaßöffnungen (9, 10) vorgesehen sind, wobei der Hauptkörper radial aufblähbar und in radial aufgeblähtem Zustand durch Fixierungsmittel (11) an der Innenseite der stromaufwärts gelegenen Arterie (2) stromaufwärts vor der Bifurkation befestigbar ist, wobei die Schenkel als separate federnde und radial expandierbare Schenkelstents (15, 16) ausgebildet sind, die in zusammengelegtem Zustand durch die abzweigenden Arterien und in die Auslaßöffnungen (9, 10) eingeführt werden können, wobei jeder der Stents (15, 16) in seinem radial expandierten Zustand gegen den Rand der entsprechenden Auslaßöffnung zur Anlage bringbar ist, um eine leckfreie, mit einer Bifurkation verse-

hene Implantationsprothese zu bilden.

2. Endovaskuläre Implantationsprothese nach Anspruch 1, dadurch gekennzeichnet, daß die Fixierungsmittel einen Hauptstent (11) umfassen, der mit dem balgförmigen Hauptkörper (8) verbunden ist, wobei ein stromabwärts gelegenes distales Ende des Hauptstents (11) durch das stromaufwärts gelegene proximale Ende des Hauptkörpers (8) überlappt wird.
3. Endovaskuläre Implantationsprothese nach Anspruch 2, dadurch gekennzeichnet, daß der Hauptstent (11) und die Schenkelstents (15, 16) durch expandierbare Metallstents gebildet sind.
4. Endovaskuläre Implantationsprothese nach einem der Ansprüche 1, 2 oder 3, dadurch gekennzeichnet, daß sich der Rand jeder Auslaßöffnung (9, 10) in Richtung stromabwärts aufweitet.
5. Endovaskuläre Implantationsprothese nach Anspruch 4, dadurch gekennzeichnet, daß der maximale Außendurchmesser jedes der Schenkelstents (15, 16) um 2 - 4 mm größer ist als der kleinste Randdurchmesser jeder Auslaßöffnung (9, 10).
6. Set, umfassend eine endovaskuläre Implantationsprothese nach einem der Ansprüche 1 - 5, wobei das Set weiter umfaßt einen ersten Führungsdraht (12) zur Verwendung bei der Einführung des Hauptkörpers (8) in eine stromaufwärts gelegene Arterie durch eine erste abzweigende Arterie (5) in Richtung stromaufwärts, um sich in einen Bereich der stromaufwärts gelegenen Arterie oberhalb der Bifurkation zu erstrecken, und zur möglichen Verwendung bei der Einführung eines Katheters durch jede der abzweigenden Arterien über jedes Ende des Führungsdrahts vor dessen Entfernung.
7. Set nach Anspruch 6, weiter umfassend einen Katheter zur Einführung durch jede der abzweigenden Arterien über jedes Ende des ersten Führungsdrahts (12) vor dessen Entfernung und zur nachfolgenden Verwendung bei der Einführung weiterer Führungsdrähte zur Verwendung bei der Einführung der Schenkelstents (15, 16).
8. Set nach Anspruch 7, weiter umfassend Führungsdrähte (13, 14) zur Verwendung bei der Einführung der Schenkelstents (15, 16).

#### Revendications

1. Prothèse pour greffe endovasculaire destinée à la mise en place sur ou à proximité d'une bifurcation dans le système artériel d'un patient et comprenant un corps principal sensiblement tubulaire (8), pour

la mise en place dans une artère amont (2), au-dessus de la bifurcation et des branches sensiblement tubulaires (15, 16), rejoignant le corps principal et étant apte à s'étendre par la bifurcation dans chacune des deux branches d'artères aval (5, 6), le corps principal étant réalisé à partir d'un matériau tissé souple microporeux et chirurgicalement implantable imperméable au sang, caractérisé en ce que le corps principal (8) est sensiblement en forme de poche avec une extrémité amont proximale ouverte et une zone de fond aval distale dans laquelle sont prévus deux dispositifs de sortie (9, 10), le corps principal étant extensible radialement et pouvant être fixé à l'état expansé radialement vers le côté interne de l'artère amont (2), en amont de la bifurcation par les moyens de fixation (11), les branches étant réalisées sous forme de dispositif dilateur (15, 16), à branches souples séparée radialement expansive pouvant être introduite à l'état escamoté dans les branches d'artères et dans les ouvertures de sorties (9, 10), chacun des dispositifs dilateurs (15, 16), pouvant être engagés dans son état expansé radialement contre le bord de l'ouverture de sortie correspondante pour assurer une prothèse de greffe bifurquée dans fuite.

2. Prothèse pour greffe endovasculaire selon la revendication 1, caractérisée en ce que les moyens de fixation comprennent un premier dispositif dilateur (11), qui est fixé sur le corps principal en forme de poche (8), avec une extrémité distale aval du dispositif dilateur principal (11), en chevauchement avec l'extrémité proximale amont du corps principal (8).
3. Prothèse pour greffe endovasculaire selon la revendication 2, caractérisée en ce que le dispositif dilateur principal (11) et les dispositifs dilateurs de branches (15, 16), sont constitués par des dilateurs métalliques expansibles.
4. Prothèse pour greffe endovasculaire selon la revendication 1, 2 ou 3, caractérisée en ce que le bord de chaque ouverture de sortie (9, 10), diverge dans la direction aval.
5. Prothèse pour greffe endovasculaire selon la revendication 4, caractérisée en ce que le diamètre externe maximum de chacun des dilateurs de branches (15, 16), est de 2-4 mm supérieur au diamètre de bord minimum de chaque ouverture de sortie (9, 10).

6. Ensemble comprenant une prothèse pour greffe endovasculaire selon l'une quelconque des revendications 1-5, cet ensemble comprenant de plus un premier fil de guidage (12) destiné à l'introduction du corps principal (8) dans une artère amont à tra-

vers une première branche d'artère (5) dans une direction amont pour s'étendre dans une zone de l'artère amont au-dessus de la bifurcation et pour l'utilisation éventuelle dans l'introduction d'un cathéter à travers chacune des branches d'artères sur chaque extrémité du fil de guidage avant son enlèvement. 5

7. Ensemble selon la revendication 6, comprenant de plus un cathéter pour l'introduction à travers chacune des branches d'artères sur chaque extrémité du premier fil de guidage (12), avant son enlèvement et pour l'utilisation ultérieure dans l'introduction d'autres fils de guidage destinés à l'introduction des dispositifs dilatateurs à branches (15, 16). 10 15

8. Ensemble selon la revendication 7 comprenant de plus des fils de guidage (13, 14), destinés à introduire les dispositifs dilatateurs à branches (15, 16). 20

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Fig. 1

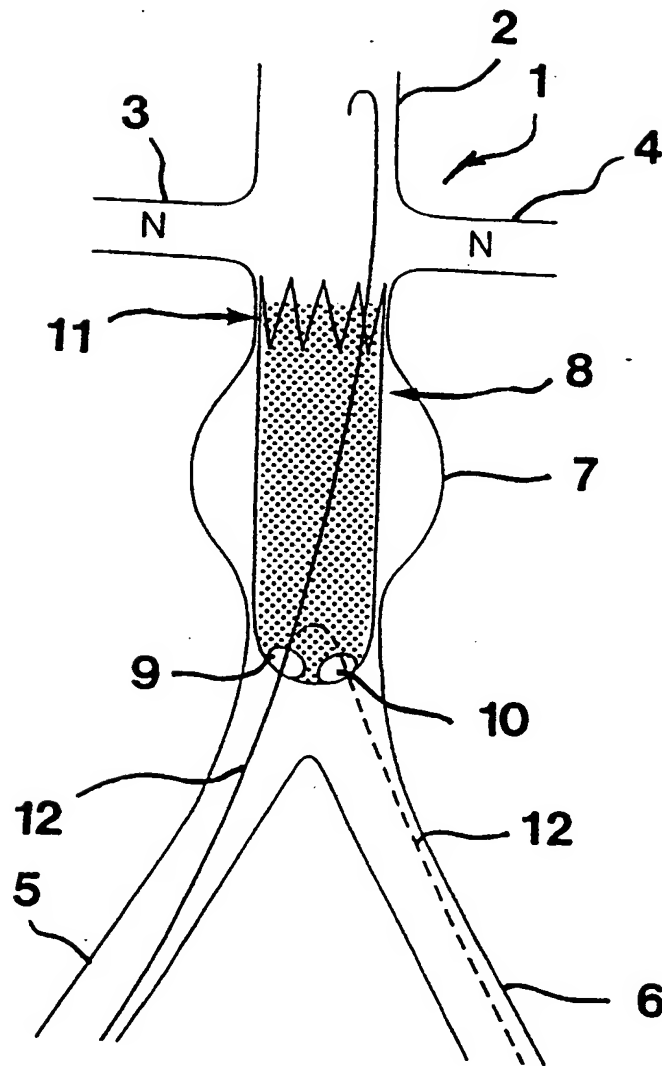
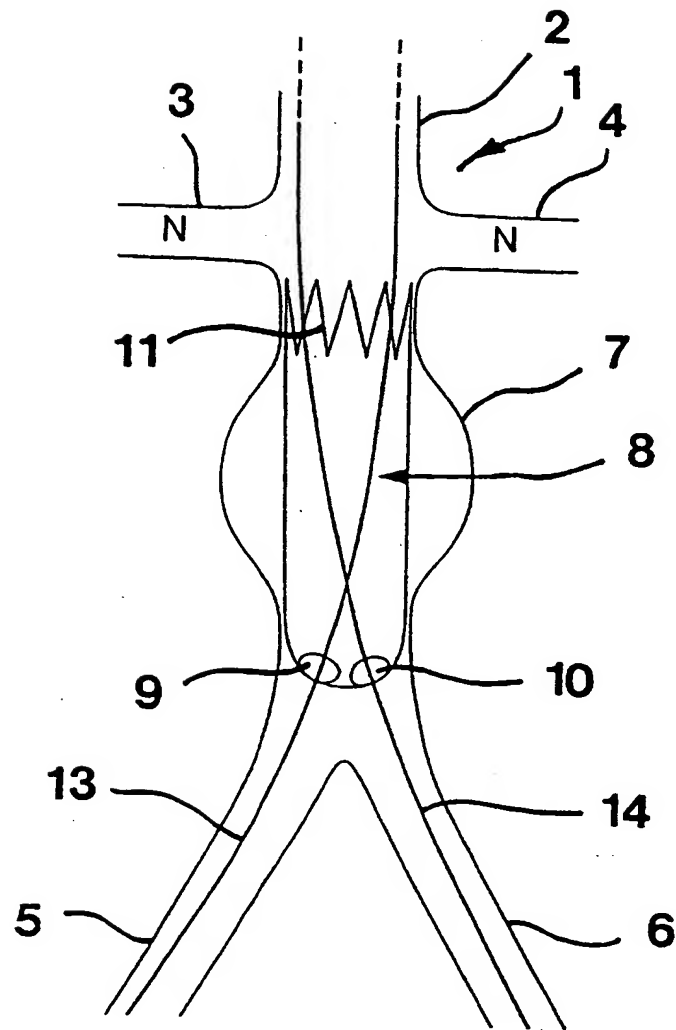
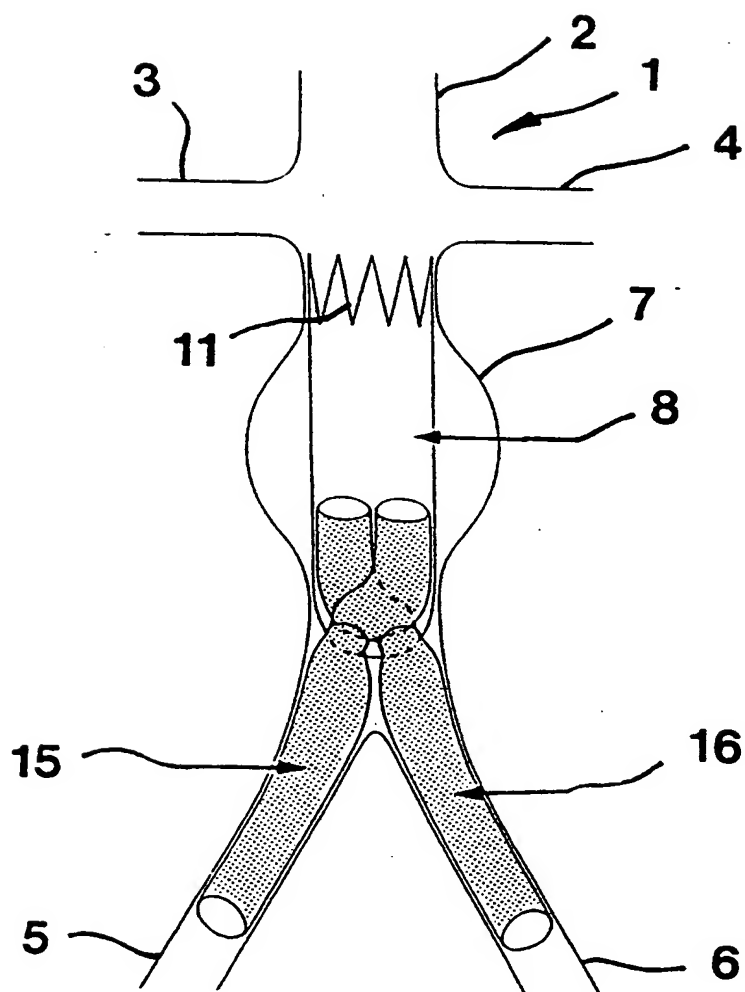


Fig. 2





**Fig. 3**



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